

Radboud University



Forward and Inverse Modeling of EEG and MEG data

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Biophysical source modelling: overview



inverse model

Overview

Motivation and background Forward modeling

Source model Volume conductor model Inverse modeling

What produces the electric current





Equivalent current dipoles



Overview

Motivation and background Forward modeling Source model **Volume conductor model** Inverse modeling

Volume conductor

described electrical properties of tissue

describes geometrical model of the head

describes **how** the currents flow, not where they originate from

same volume conductor for EEG as for MEG, but also for tDCS, tACS, TMS, ...



Volume conductor

Computational methods for volume conduction problem that allow for realistic geometries

- BEM Boundary Element Method
- FEM Finite Element Method
- FDM Finite Difference Method

Volume conductor: Boundary Element Method

Each compartment is homogenous isotropic

Important tissues skin skull brain (CSF)

Triangulated surfaces describe boundaries



Volume conductor: Boundary Element Method

Construction of geometry

segmentation in different tissue types

extract surface description

downsample to reasonable number of triangles







Volume conductor: Boundary Element Method

Construction of geometry segmentation in different tissue types extract surface description downsample to reasonable number of triangles Computation of model independent of source model only one lengthy computation fast during application to real data Can also include more complex geometrical details ventricles holes in skull

Volume conductor: Finite Element Method

Tesselation of 3D volume in tetraeders or hexaheders







Volume conductor: Finite Element Method





tetraeders

hexaheders

Volume conductor: Finite Element Method

Tesselation of 3D volume in tetraeders or hexaheders



Each element can have its own conductivity

FEM is the most accurate numerical method but computationally quite expensive

Geometrical processing not as simple as BEM

Volume conductor: Finite Difference Method



Volume conductor: Finite Difference Method



$$\Delta V_1 / R_1 + \Delta V_2 / R_2 + \Delta V_3 / R_3 + \Delta V_4 / R_4 = 0$$

$$\Delta \mathbf{v}_1 / \mathbf{x}_1 + \Delta \mathbf{v}_2 / \mathbf{x}_2 + \Delta \mathbf{v}_3 / \mathbf{x}_3 + \Delta \mathbf{v}_4 / \mathbf{x}_4 = \mathbf{0} = \mathbf{0}$$

 $(V_1-V_0)/R_1 + (V_2-V_0)/R_2 + (V_3-V_0)/R_3 + (V_4-V_0)/R_4 = 0$

Volume conductor: Finite Difference Method

Unknown potential Vi at each node Linear equation for each node approx. 100x100x100 = 1.000.000 linear equations just as many unknown potentials

Add a source/sink

sum of currents is zero for all nodes, except sum of current is I+ for a certain node sum of current is I- for another node

Solve for unknown potential

EEG volume conduction



EEG volume conduction

Potential difference between electrodes corresponds to current flowing through skin

Only tiny fraction of current passes through skull

Therefore the model should describe the skull and skin as accurately as possible

MEG volume conduction

MEG measures magnetic field over the scalp



MEG volume conduction compared to EEG

EEG is measurement on scalp potential difference due to volume currents

MEG field not affected by head

- magnetic field due to primary current (source)
- magnetic field due to secondary (volume) currents



Overview

Motivation and background Forward modeling Source model Volume conductor model EEG versus MEG Inverse modeling

Biophysical source modelling: overview

forward model



Inverse localization: demo



Inverse methods

Single and multiple dipole models

Minimize error between model and measured potential/field

Distributed source models

Perfect fit of model to the measured potential/field Additional constraint on source smoothness, power or amplitude

Spatial filtering

Scan the whole brain with a single dipole and compute the filter output at every locationBeamforming (e.g. LCMV, SAM, DICS)Multiple Signal Classification (MUSIC)