

## **Radboud University**



# Introduction to EEG, MEG and analysis with the FieldTrip toolbox

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#### What is FieldTrip

a MATLAB toolbox for the analysis of MEG, EEG and animal electrophysiology data

can import data from many different file formats

contains algorithms for spectral analysis, source reconstruction, statistics, connectivity, ...

#### Talk outline

What kind of signals are generated in the brain

How do we record those signals

Analyzing those signals with FieldTrip

Background on the FieldTrip toolbox

#### Talk outline

What kind of signals are generated in the brain

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Analyzing those signals with FieldTrip

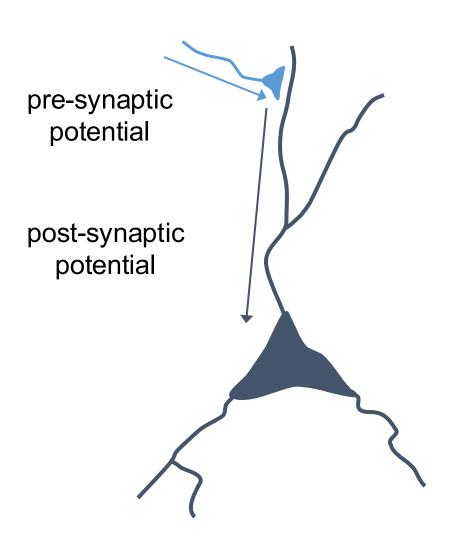
Background on the FieldTrip toolbox

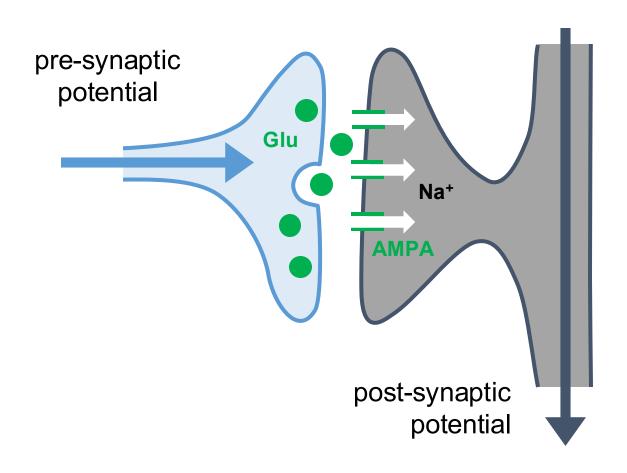
What kind of signals are generated in the brain

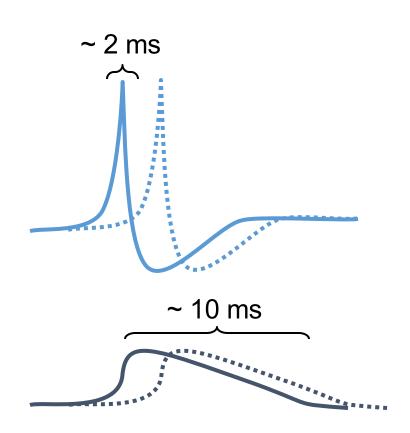
We measure the scalp potentials or field associated with post-synaptic potentials in pyramidal neurons

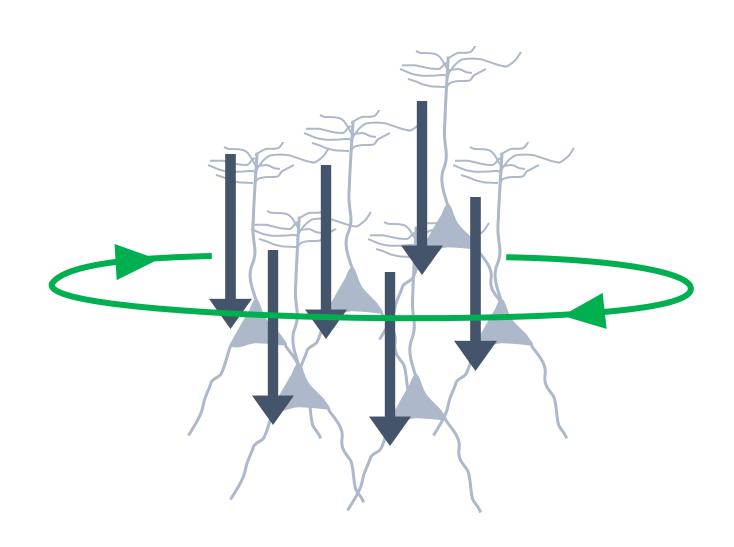
These PSPs represent the exitatory and inhibitory input that these neurons receive

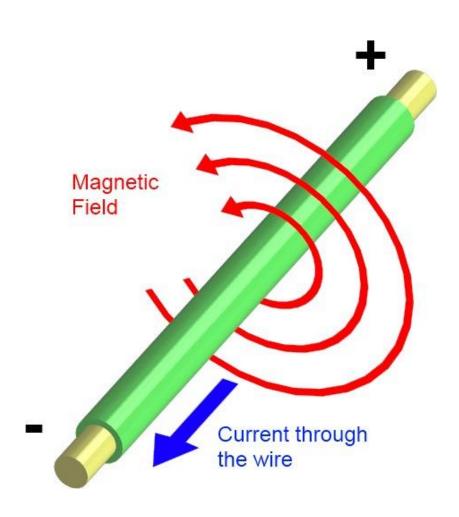
Usually we study this neuronal input following the presentation of a stimulus or following a cognitive event

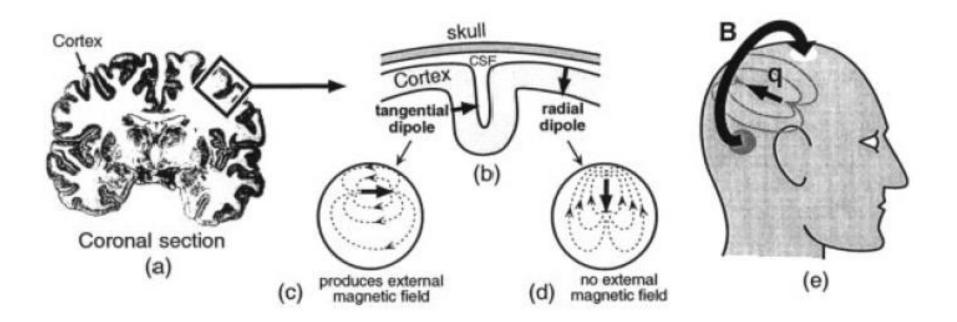




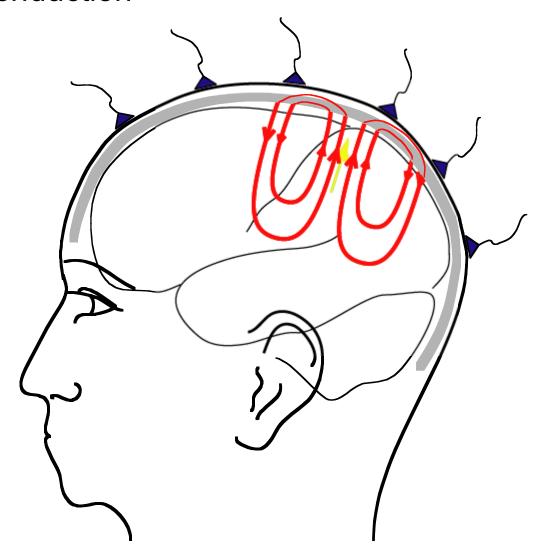




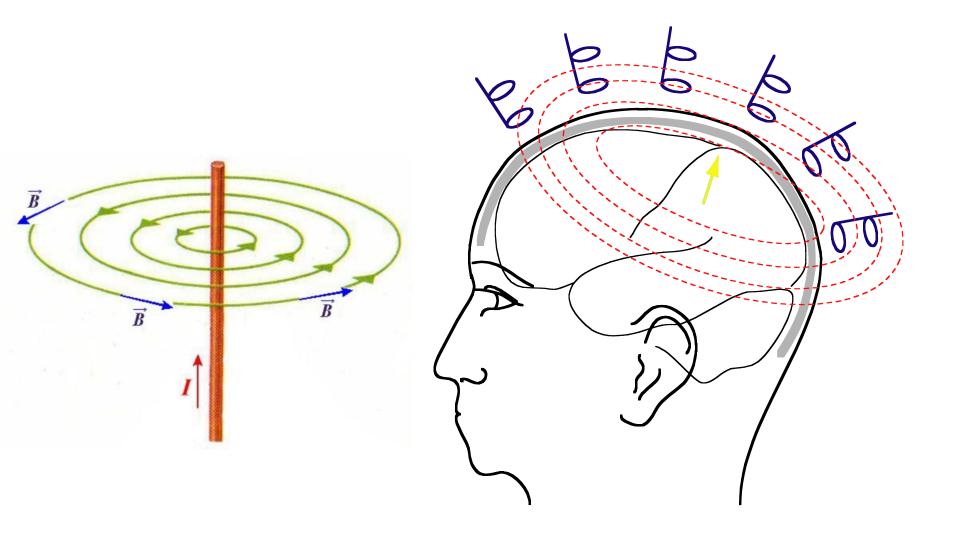




#### EEG volume conduction



# Electric current → magnetic field



#### Talk outline

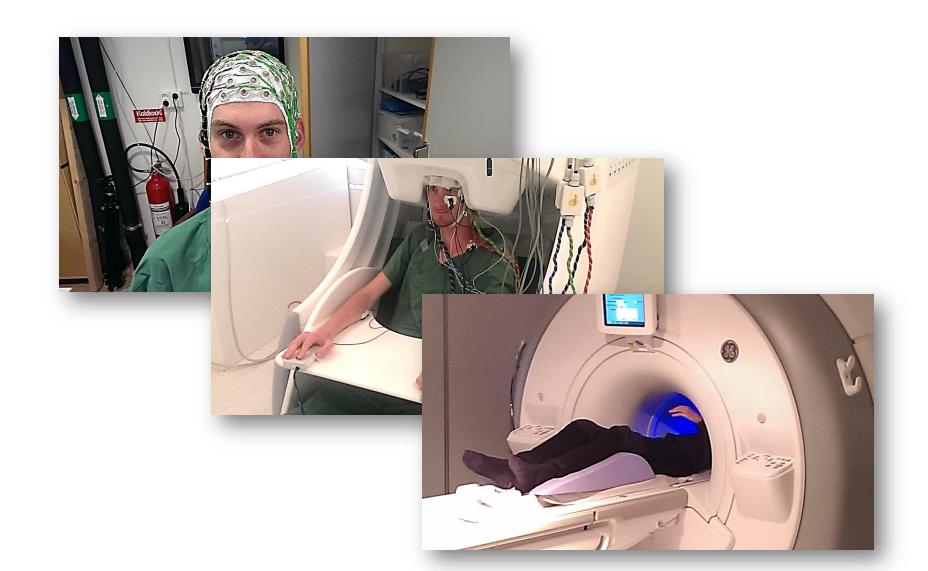
What kind of signals are generated in the brain

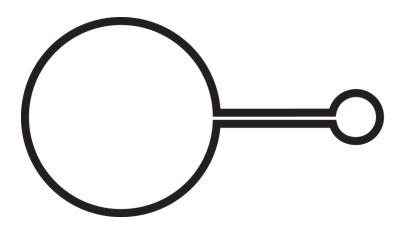
How do we record those signals

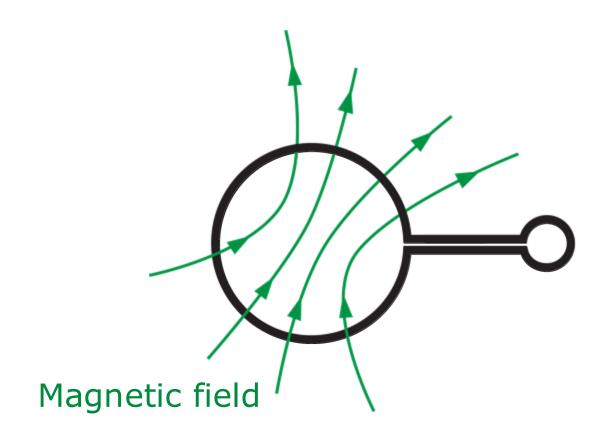
Analyzing those signals with FieldTrip

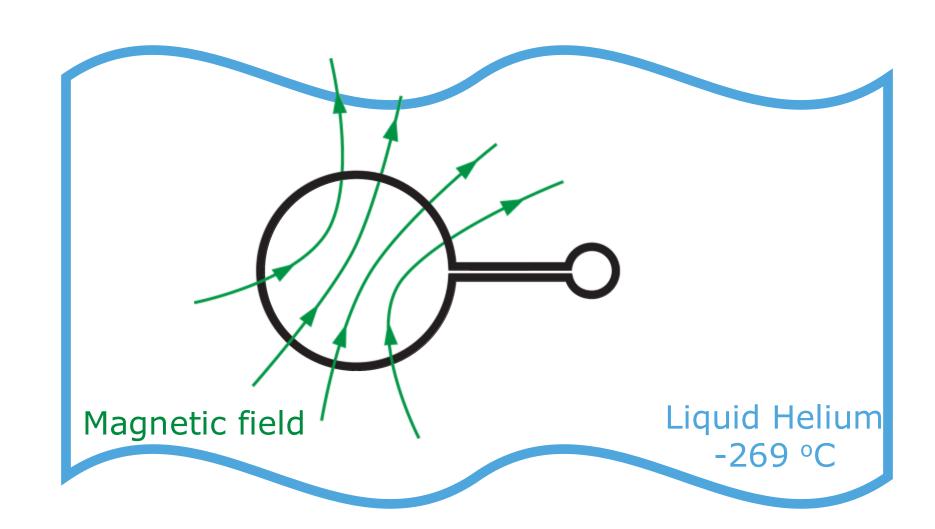
Background on the FieldTrip toolbox

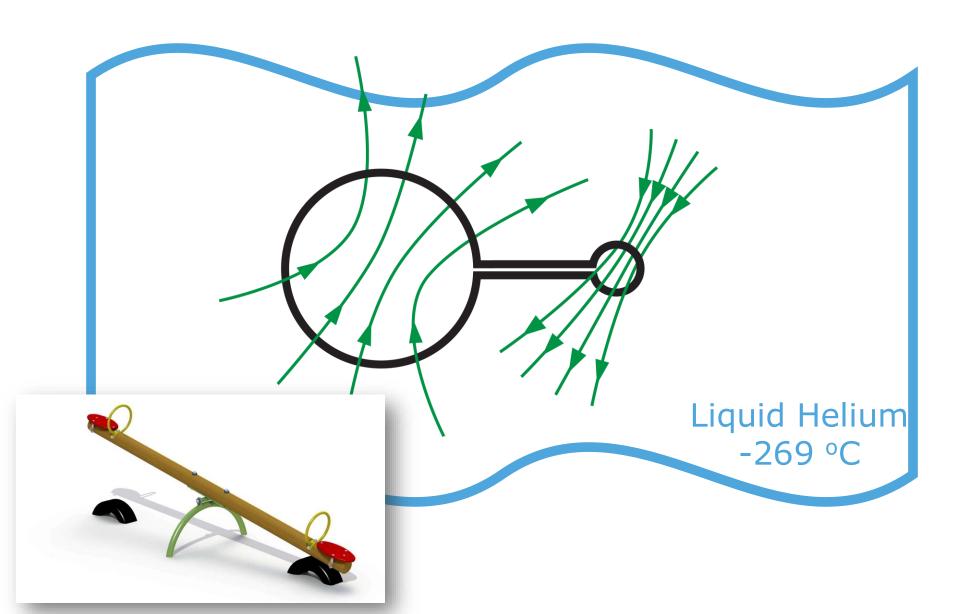
### How do we record these signals from the brain

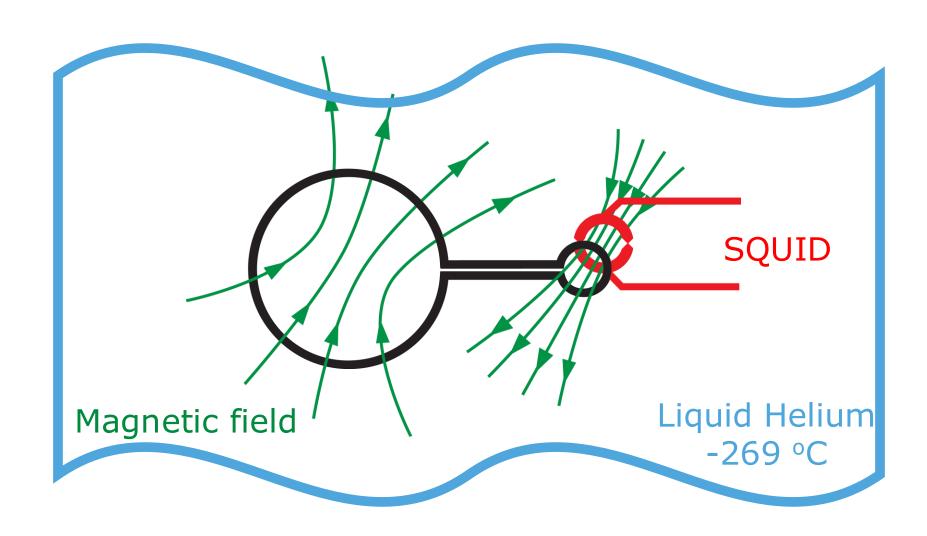




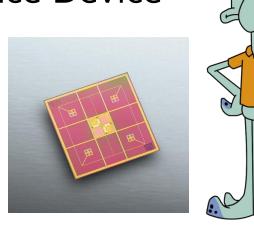


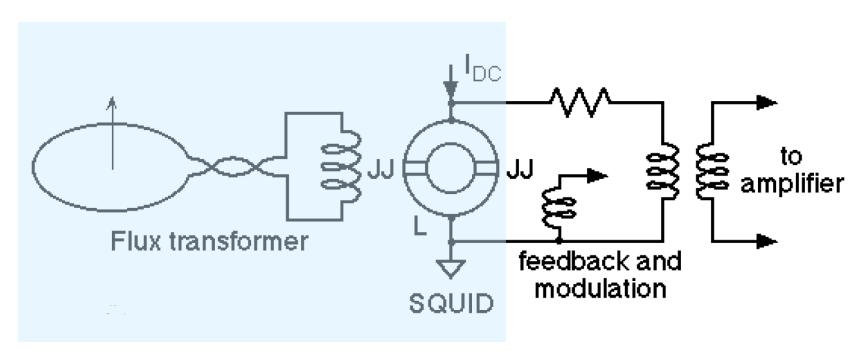






# Magnetic field detectors Superconducting QUantum Interference Device





# Magnetic field strength - compared

100	1.5 - 3 T	MRI systems
<b>10</b> <sup>-3</sup>	5 mT	typical refrigerator magnet
10-6	30-60 uT	earth's magnetic field
10-9	0.1 -10 nT	heliosphere
10-12	0.1 - 1.0 pT	spontaneous brain activity
10-15	10-100 fT	ERF differences

#### Technical challenges of MEG

Requires sensitive magnetic detectors

Deal with environmental noise
shielding
sensor design
reference sensors for noise subtraction

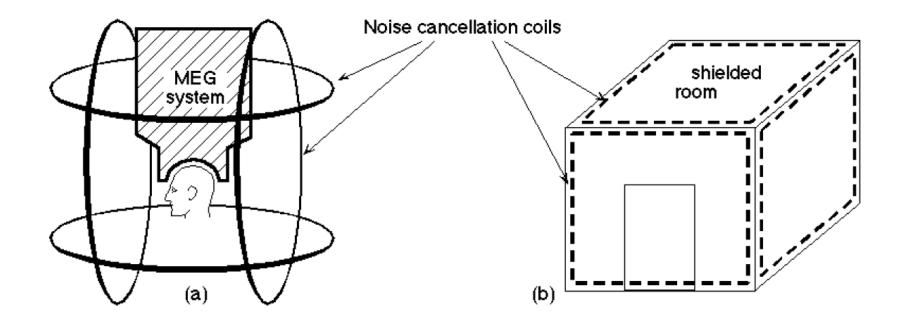
### Shielding - passive

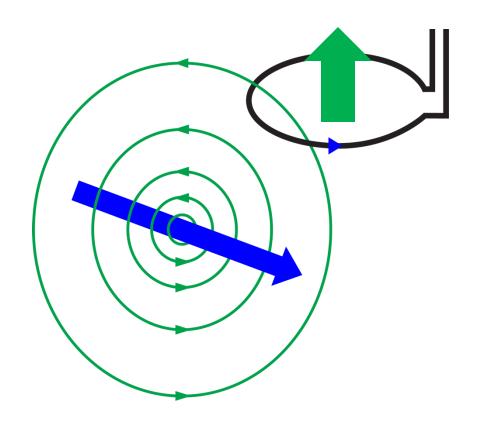


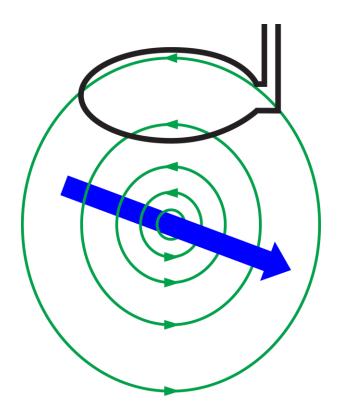
The magnetically shielded room built by David Cohen at MIT's Francis Bitter National Magnet Laboratory in 1969.

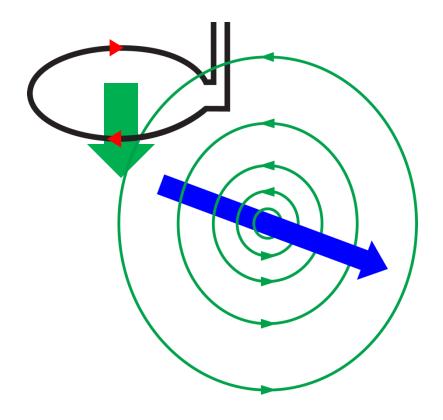


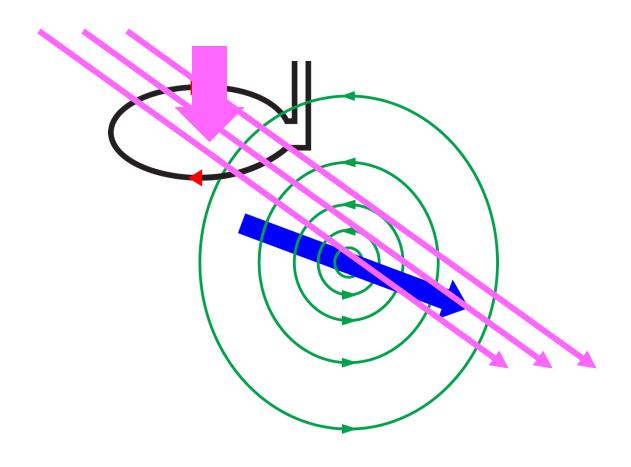
### Shielding - active

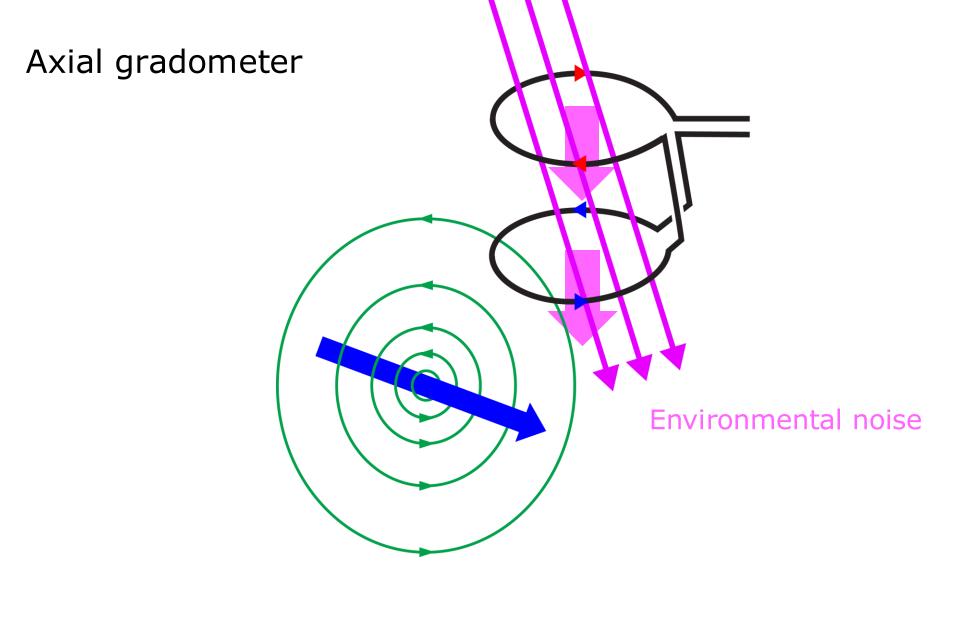




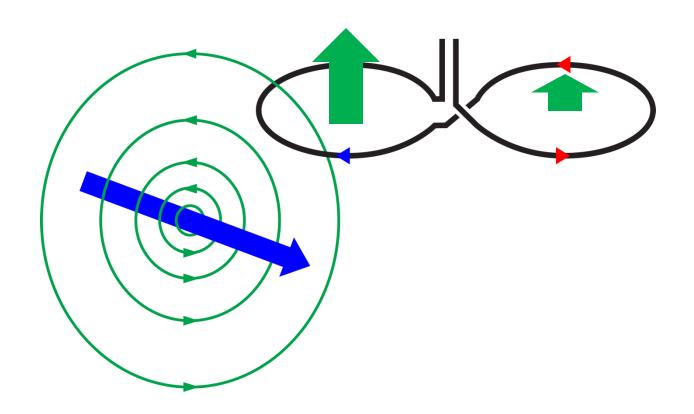


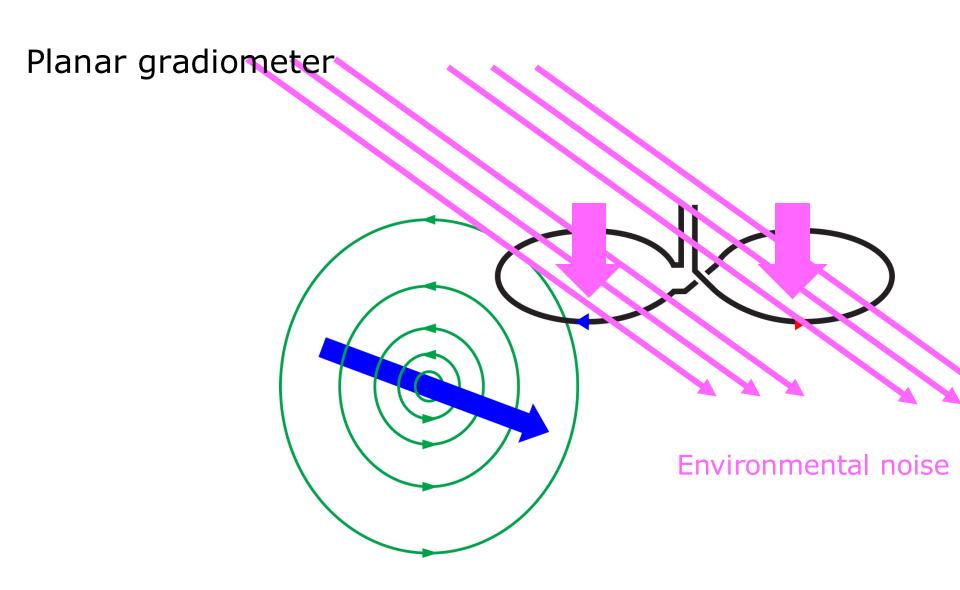




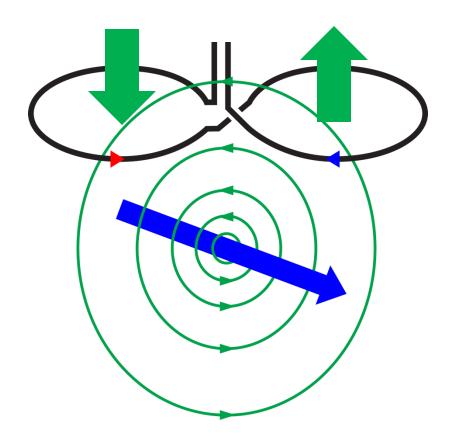


# Planar gradiometer

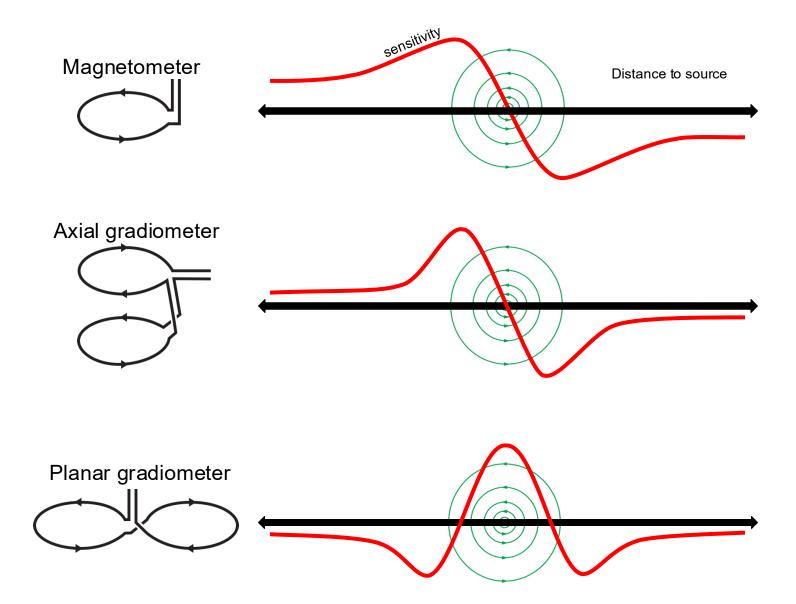


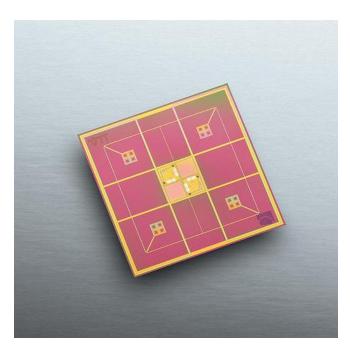


# Planar gradiometer



#### MEG sensor – sensitivity profile



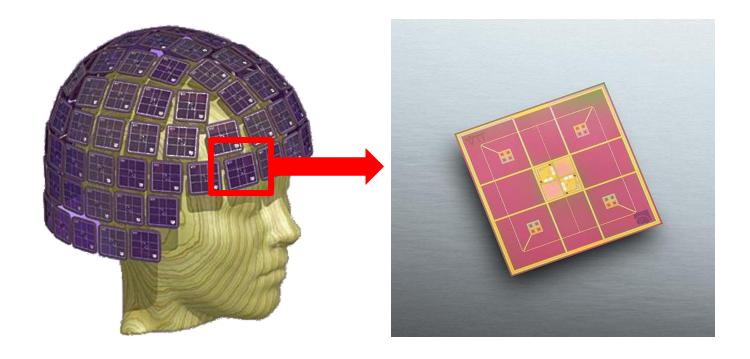


# Neuromag/Elekta/Megin

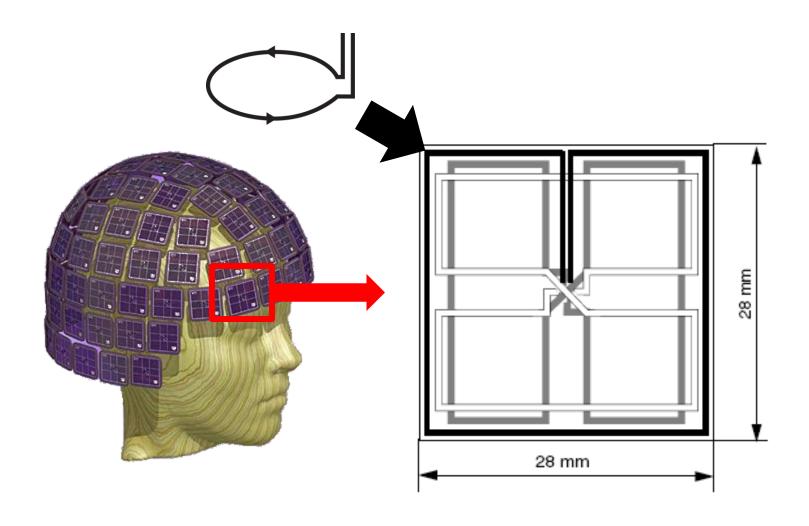
102 magnetometers204 planar gradiometers306 channels total



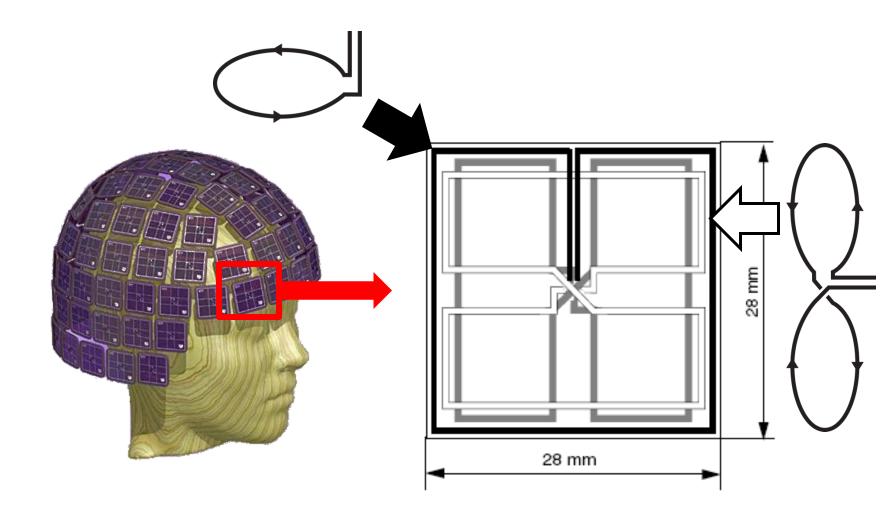
# Neuromag/Elekta/Megin



# Neuromag/Elekta/Megin



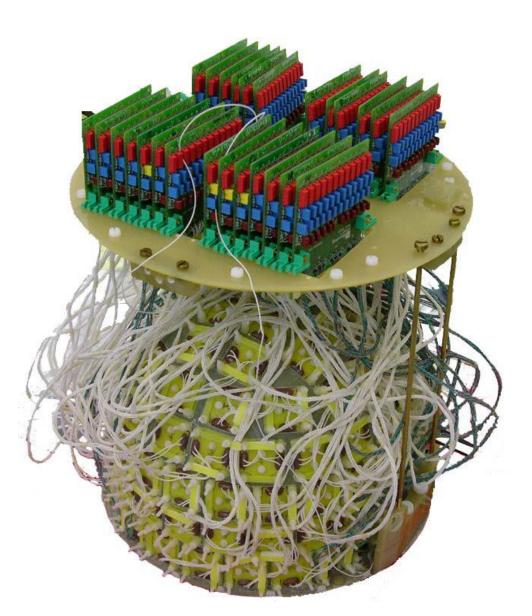
# Neuromag/Elekta/Megin



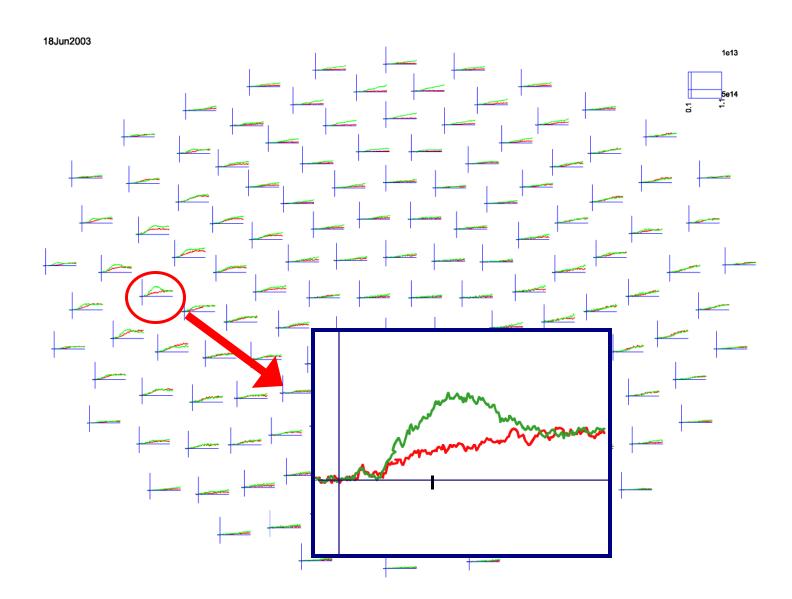
# Neuromag/Elekta/Megin 28 mm 28 mm

# Neuromag/Elekta/Megin

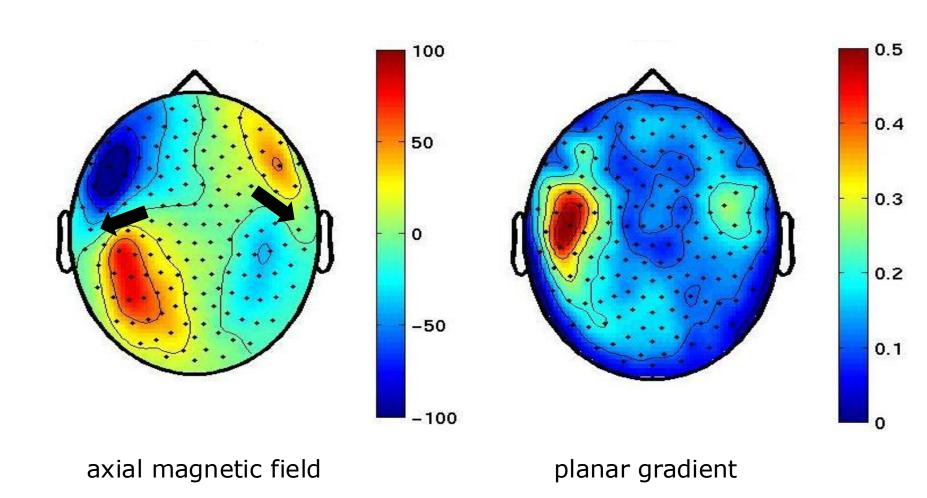




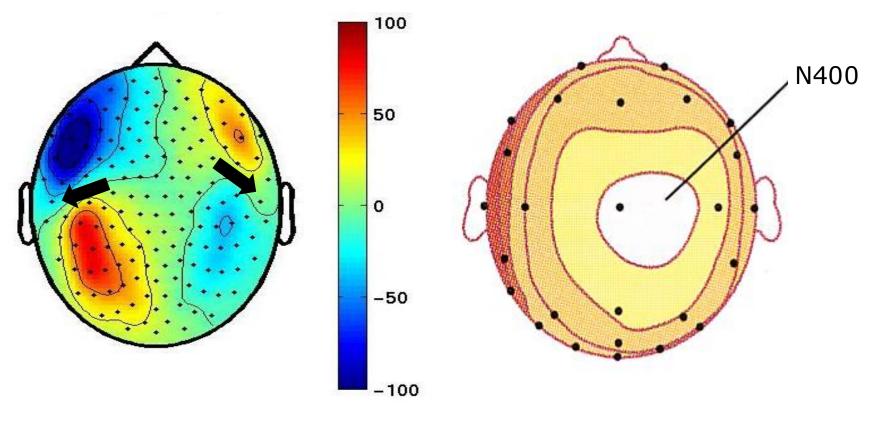
# N400 response in MEG



## N400 response - compared between MEG systems



#### N400 response - compared between MEG and EEG



axial magnetic field

potential distribution

#### **LETTER**

# Moving magnetoencephalography towards real-world applications with a wearable system

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Imaging human brain function with techniques such as magnetoencephalography typically requires a subject to perform tasks while their head remains still within a restrictive scanner. This artificial environment makes the technique inaccessible to many people, and limits the experimental questions that can be addressed. For example, it has been difficult to apply neuroimaging to investigation of the neural substrates of cognitive development in babies and children, or to study processes in adults that require unconstrained head movement (such as spatial navigation). Here we describe a magnetoencephalography system that can be worn like a helmet, allowing free and natural movement during scanning. This is possible owing to the integration of quantum sensors<sup>2,3</sup>, which do not rely on superconducting technology, with a system for nulling background magnetic fields. We demonstrate human electrophysiological measurement at millisecond resolution while subjects make natural movements, including head nodding,

stretching, drinking and playing a ball game. Our results compare well to those of the current state-of-the-art, even when subjects make large head movements. The system opens up new possibilities for scanning any subject or patient group, with myriad applications such as characterization of the neurodevelopmental connectome, imaging subjects moving naturally in a virtual environment and investigating the pathophysiology of movement disorders.

Magnetoencephalography<sup>1</sup> (MEG) allows direct imaging of human brain electrophysiology by measurement of magnetic fields generated at the scalp by neural currents. Mathematical analysis of those fields enables the generation of 3D images that show the formation and dissolution of brain networks in real time. MEG measurements of brain activity are currently made using an array of superconducting sensors placed around the head<sup>1-4</sup>. These cryogenically cooled sensors have femtotesla (fT) sensitivity, which is needed to detect the weak magnetic fields produced by the brain. Unfortunately, the requirement

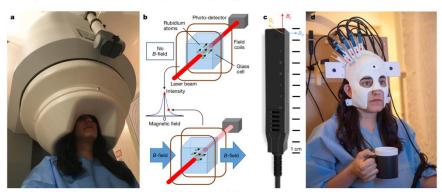


Figure 1 | A new generation of MEG system. a, A conventional 275-channel cryogenic MEG system. Weighing about 450 kg, the system is fixed and cumbersome and subjects must remain still relative to the fixed sensor array. b, Schematic illustration of zero-field resonance in an OPM sensor. Top, operation in zero-field; bottom, Larmor precession when an external field (*B*-field) impinges on the cell and the transmitted light intensity is reduced. c, A commercial OPM sensor made by QuSpin. The geometry used is illustrated by the coloured axes where *B*<sub>i</sub> is the radial

field component, B, the tangential field component and B, the direction along which the laser beam is oriented. d. Our prototype OPM-MEG system helmet. The helmet weighs 905 g and is customized so that the sensors (which in this prototype cover only the right sensorimotor cortex) are directly adjacent to the scalp surface. The subject is free to move their head. The measured radial field direction for the sensors is illustrated by the red arrows.

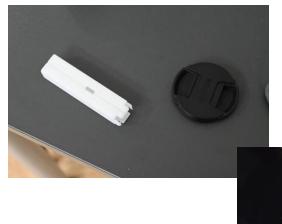
Sir Peter Mansfield Imaging Centre, School of Physics and Astronomy, University of Nottingham, University Park, Nottingham NG7 2RD, UK. <sup>2</sup>Outspin Inc., 331 South 104th Street, Suite 130, Louisville, Colorado 80027, USA. <sup>3</sup>Wellicome Centre for Human Neuroimaging, UCL institute of Neurology, University College London, 12 Queen Square, London WC1N 3BG, UK. <sup>4</sup>Institute of Cognitive Neuroscience, University College London, 17–19 Queen Square, London WC1N 3AZ, UK. <sup>4</sup>Centre for Human Brain Health, School of Psychology, University of Birmingham, Edgbaston, Birmingham B15 2TT, UK. <sup>4</sup>Sobell Department for Motor Neuroscience and Movement Disorders, UCL Institute of Neurology, University College London, Queen Square House, Queen Square, London WC1N 3BG, UK.

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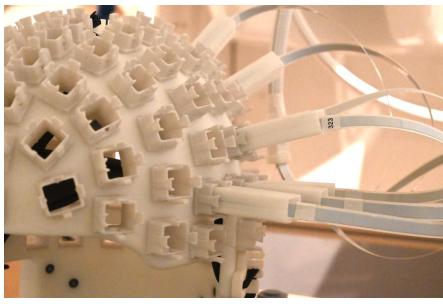
<sup>\*</sup>These authors contributed equally to this work. §These authors jointly supervised this work.



# FieldLine OPM system in Stockholm

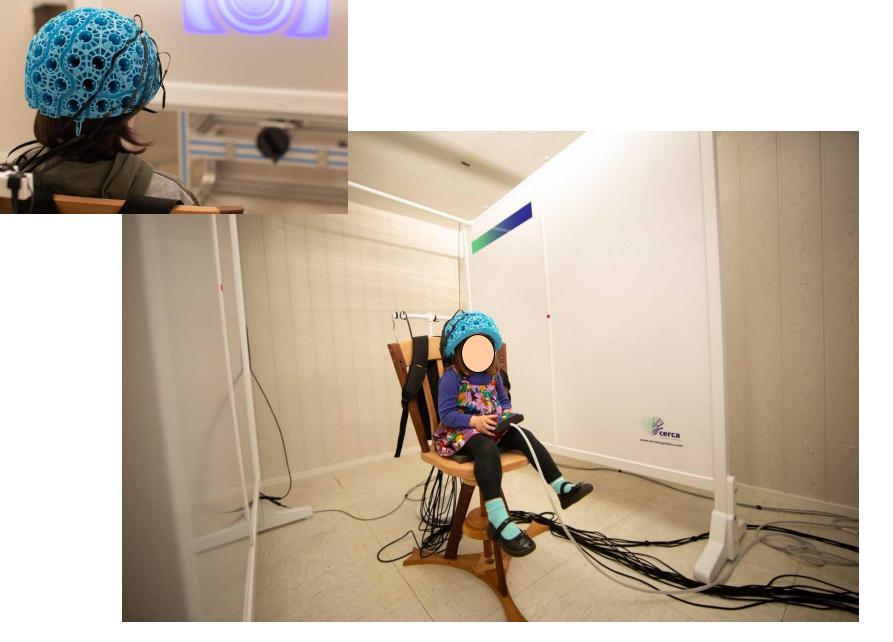




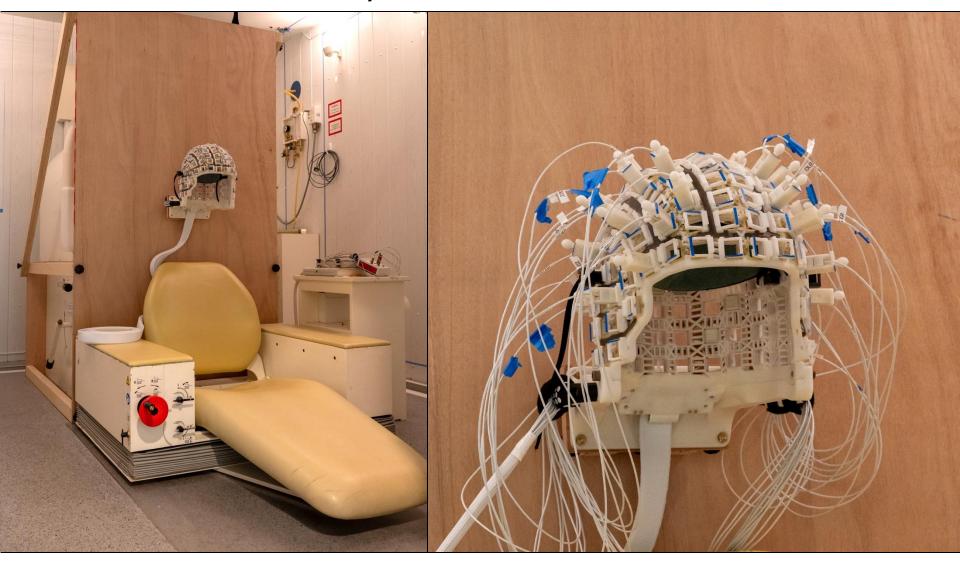


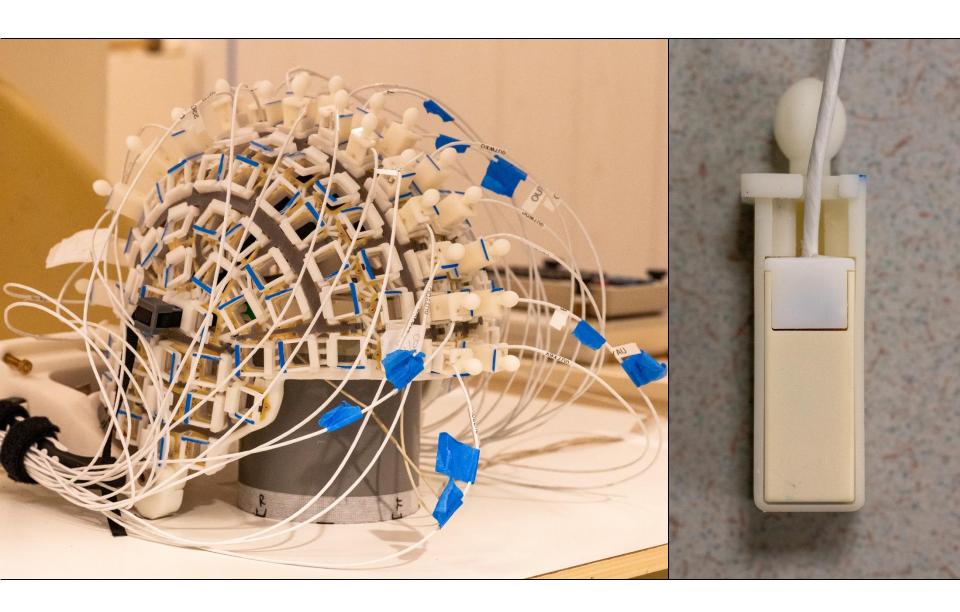




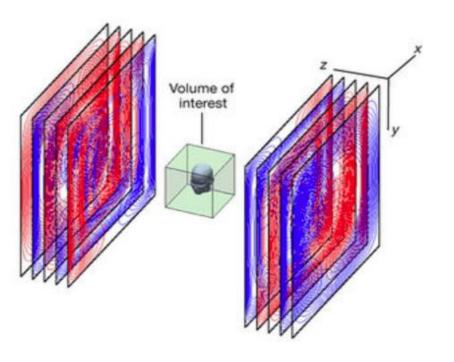


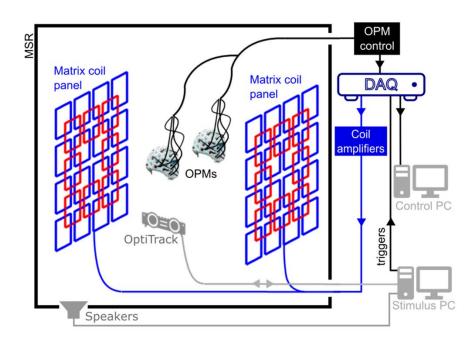
# 32 sensor FieldLine system installed at DCCN





## Ambient field nulling coils





Bi-planar coils

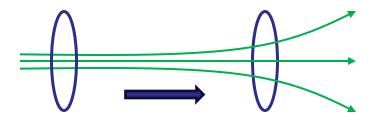
Matrix coils

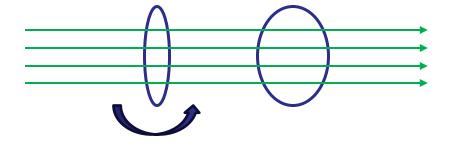
# Simple Helmholz-style coils in our MSR

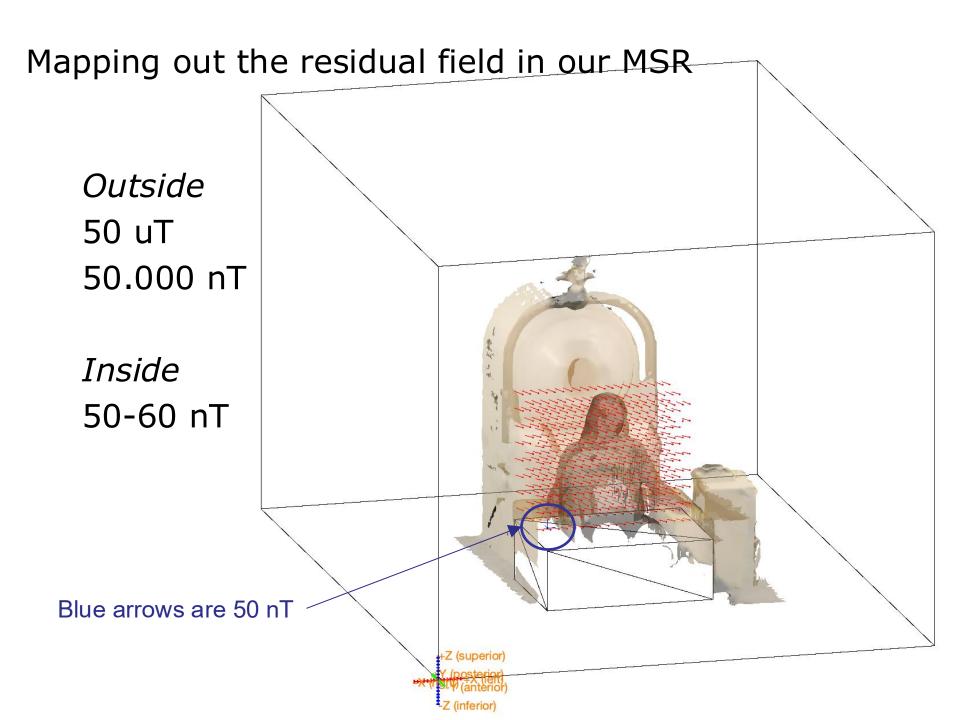




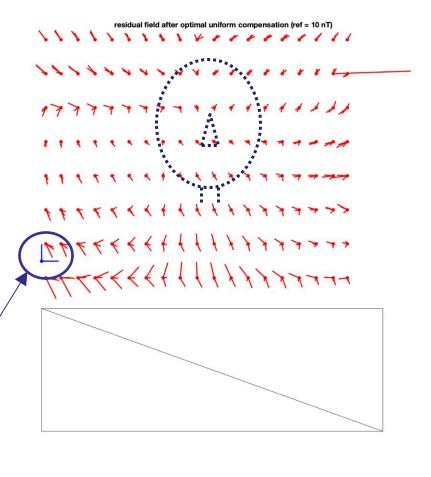
# OPM magnetometer movements pick up residual magnetic fields and gradients





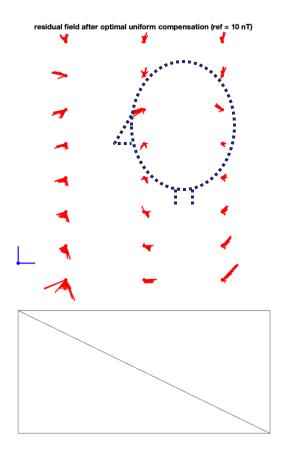


#### Residual gradient – seen from front



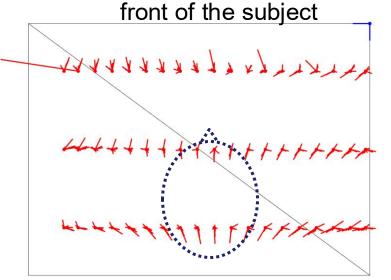
Blue arrows are 10 nT

# Residual gradient – seen from left



#### Residual gradient – seen from top

residual field after optimal uniform compensation (ref = 10 nT)



right of the subject

#### Talk outline

What kind of signals are generated in the brain

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Analyzing those signals with FieldTrip

Background on the FieldTrip toolbox

#### M/EEG signal characteristics considered during analysis

timecourse of activity

-> ERP

spectral characteristics

-> power spectrum

temporal changes in power

-> time-frequency response (TFR)

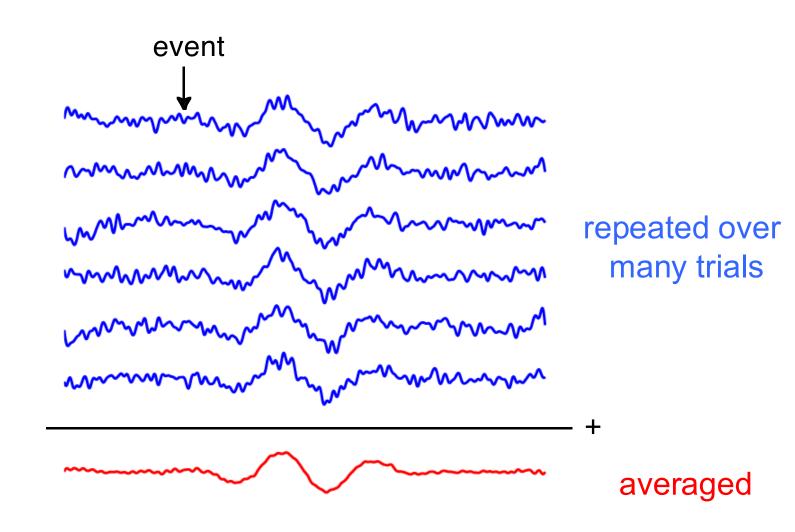
spatial distribution of activity over the head

-> source reconstruction

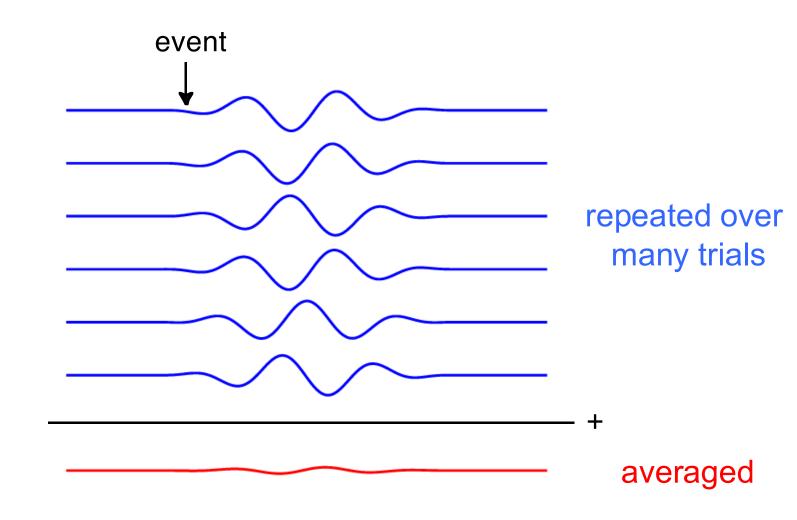
# Evoked activity

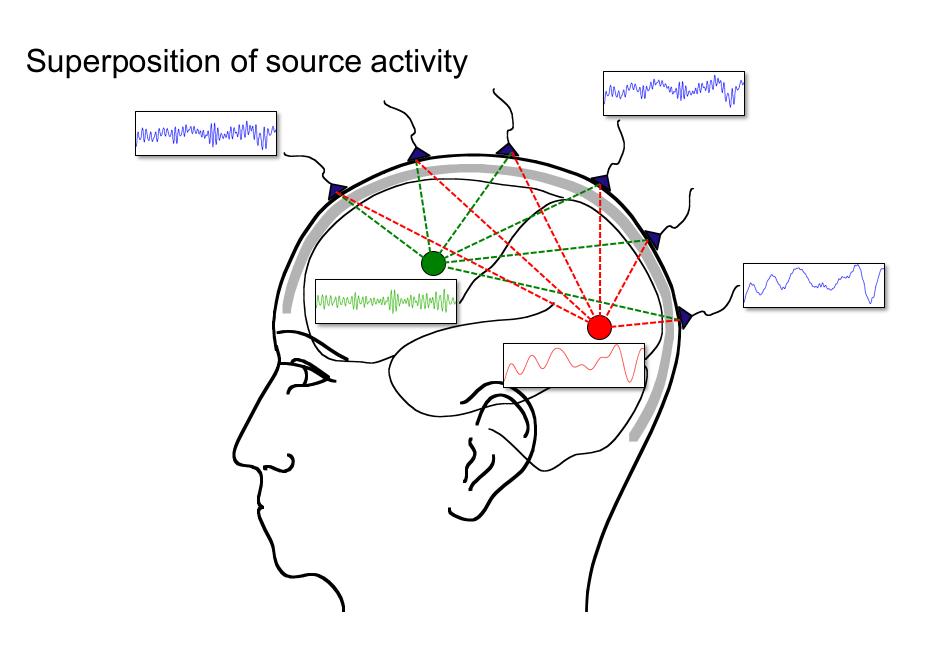


### **Evoked activity**



## Induced activity





#### Separating activity of sources

# Use the temporal aspects of the data at the channel level

**ERF** latencies

ERF difference waves

Filtering the time-series

Spectral decomposition

#### Use the spatial aspects of the data

Volume conduction model of head

Estimate source model parameters

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#### Some FieldTrip basics



the "cfg" argument is a contiguration structure, e.g.

```
cfg.channel = {'C3', C4', 'F3', 'F4'}
cfg.foilim = [1 70]
```

#### FieldTrip v.s. default Matlab

dataout = functionname(cfg, datain, ...)

cfg.key1 = value1 cfg.key2 = value2

dataout = functionname(datain, key1, value1, ...)

#### Using functions in an analysis protocol

# ft\_preprocessing

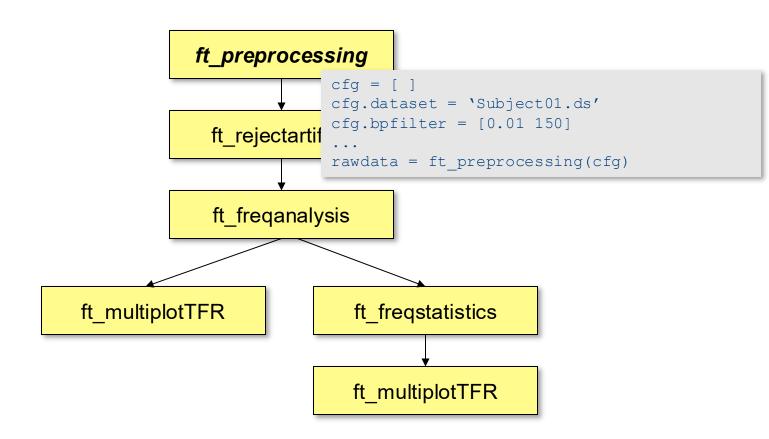
FT\_PREPROCESSING reads MEG and/or EEG data according to user-specified trials and applies several user-specified preprocessing steps to the signals.

```
Use as
  [data] = ft_preprocessing(cfg)
or
  [data] = ft_preprocessing(cfg, data)
```

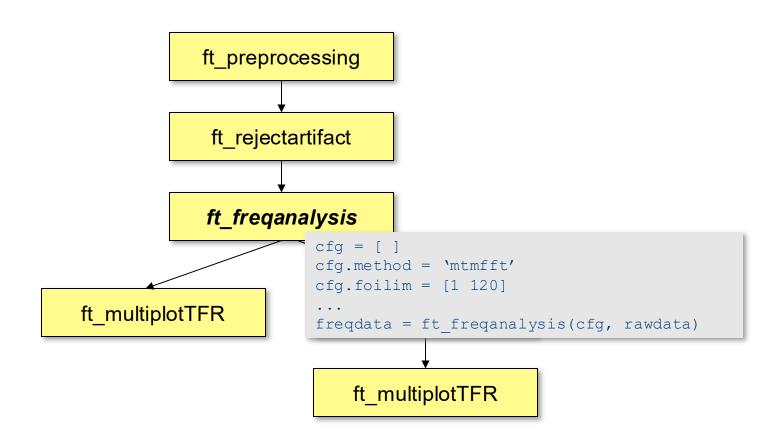
The first input argument "cfg" is the configuration structure, which contains all details for the dataset filenames, trials and the preprocessing options. You can only do preprocessing after defining the segments of data to be read from the file (i.e. the trials), which is for example done based on the occurence of a trigger in the data.

. . .

#### Using functions in an analysis protocol



#### Using functions in an analysis protocol



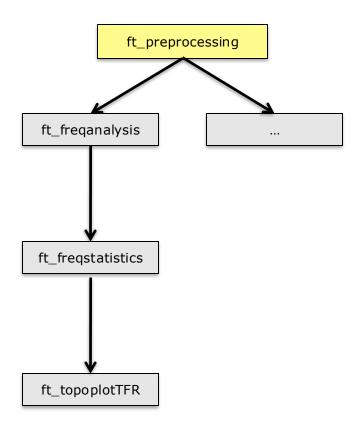
#### Raw data structure

```
rawData =
    label: {151x1 cell}
    trial: {1x80 cell}
    time: {1x80 cell}
    fsample: 300
    hdr: [1x1 struct]
    cfg: [1x1 struct]
```

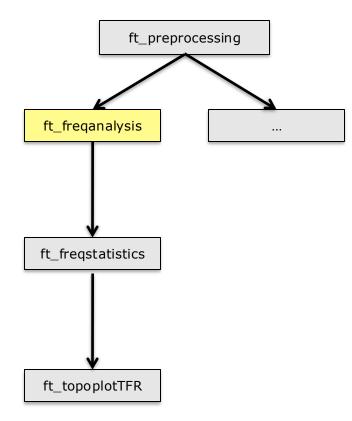
#### Event related response

```
timelockData =
    label: {151x1 cell}
    avg: [151x900 double]
    var: [151x900 double]
    time: [1x900 double]
    dimord: 'chan_time'
    cfg: [1x1 struct]
```

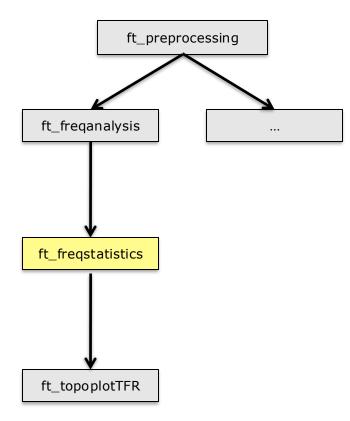
```
cfq = []
cfq.dataset = 'Subject01.ds'
cfg.bpfilter = [0.01 150]
rawdata = ft preprocessing(cfg)
```

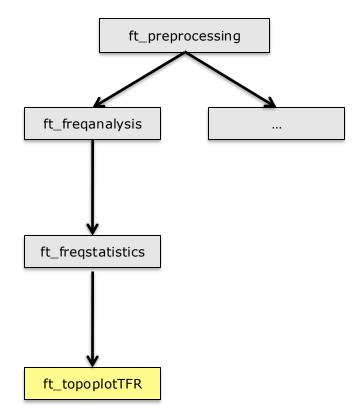


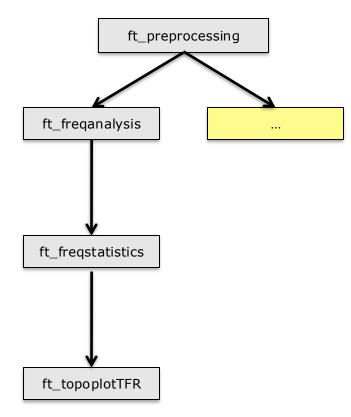
```
cfg = []
cfq.method = 'mtmfft'
cfg.foilim = [1 120]
freqdata = ft freqanalysis(cfg, rawdata)
```



```
cfq = []
cfg.method = 'montecarlo'
cfg.statistic = 'indepsamplesT'
cfg.design = [1 2 1 2 2 1 2 1 1 2 ...]
freqstat = ft freqstatistics(cfg, freqdata)
```







```
subj = { 'S01.ds', 'S02.ds', ...}
trig = [1 \ 3 \ 7 \ 9]
for s=1:nsubj
for c=1:ncond
 cfq = []
  cfg.dataset = subj{s}
  cfg.trigger = trig(c)
  rawdata{s,c} = ft preprocessing(cfg)
  cfg = []
  cfg.method = 'mtmfft'
  cfg.foilim = [1 120]
  freqdata(s,c) = ft freqanalysis(cfg, rawdata(s,c))
end
end
```

```
subj = { 'S01.ds', 'S02.ds', ...}
triq = [1 \ 3 \ 7 \ 9]
for s=1:nsubj
for c=1:ncond
 cfq = []
  cfg.dataset = subj{s}
  cfg.trigger = trig(c)
  rawdata = ft preprocessing(cfg)
  filename = sprintf('raw%s %d.mat', subj{s}, trig(c));
  save(filename, 'rawdata')
end
end
```

# Example use in distributed computing

```
subj = { 'S01.ds', 'S02.ds', ...}
trig = [1 \ 3 \ 7 \ 9]
for s=1:nsubj
for c=1:ncond
  cfqA\{s,c\} = []
  cfgA\{s,c\}.dataset = subj\{s\}
  cfgA{s,c}.trigger = trig(c)
  cfqA{s,c}.outputfile = sprintf('raw%s %d.mat', subj{s}, trig(c))
  cfgB\{s,c\} = []
  cfgB{s,c}.dataset = subj{s}
  cfgB{s,c}.trigger = trig(c)
  cfgB{s,c}.inputfile = sprintf('raw%s %d.mat', subj{s}, trig(c));
  cfgB{s,c}.outputfile = sprintf('freq%s %d.mat', subj{s}, trig(c));
end
end
dfeval(@ft preprocessing, cfgA)
dfeval(@ft_freqanalysis, cfgB)
```

# Example use in distributed computing

```
subj = { 'S01.ds', 'S02.ds', ...}
trig = [1 \ 3 \ 7 \ 9]
for s=1:nsubj
for c=1:ncond
  cfqA\{s,c\} = []
  cfgA\{s,c\}.dataset = subj\{s\}
  cfgA\{s,c\}.trigger = trig(c)
  cfqA{s,c}.outputfile = sprintf('raw%s %d.mat', subj{s}, trig(c))
  cfgB\{s,c\} = []
  cfgB{s,c}.dataset = subj{s}
  cfgB{s,c}.trigger = trig(c)
  cfgB{s,c}.inputfile = sprintf('raw%s %d.mat', subj{s}, trig(c));
  cfgB{s,c}.outputfile = sprintf('freq%s %d.mat', subj{s}, trig(c));
end
end
qsubcellfun(@ft preprocessing, cfgA)
qsubcellfun(@ft_freqanalysis,
                                cfqB)
```

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Background on the FieldTrip toolbox

# FieldTrip is a toolbox

the data and the separate functions are in your hands

the scripts depend on the data properties, your computer and on your programming skills and style

scripts correspond to analysis protocols

scripts can be reviewed by supervisors scripts are often shared with colleagues scripts can be published/released

# Finding your way around in the FieldTrip toolbox

### Matlab

help functionname edit functionname

### Website

http://www.fieldtriptoolbox.org

Email discussion list

Expertise in your local group



# **Radboud University**



# Introduction to EEG, MEG and analysis with the FieldTrip toolbox

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